

FENG Distinguished Lecture Department of Biomedical Engineering Hong Kong PolyU 24th June, 2019

Nanoparticle-mediated tissue imaging and therapy at the intersection of light and sound

Ronald A. Roy Department of Engineering Science The University of Oxford



- High-intensity focused ultrasound (HIFU) is helpful in therapeutic medical procedures
- Primary bioeffect is tissue heating from ultrasound absorption
- Acoustic cavitation can enhance HIFU efficacy by accelerating heating and promoting mechanical damage

What is Acoustic Cavitation?



Acoustic Cavitation A Recipe...

Start with a preferential site for liquid rupture

Imperfectly wetted solid, preexisting gas cavity, superheated nanodroplet, etc.

Apply an acoustic stress strong enough to overcome...

Surface tension, inertia, viscous drag

A microbubble is formed that pulsates radially in response to periodic acoustic forcing

Acoustic Cavitation



Force balance across a bubble wall

- △*F* = *ma*
- Internal: gas pressure vapor pressure
- External: hydrostatic pressure, surface tension

Rayleigh Plesset Equation

1-D radial motion, Newtonian incompressible fluid

$$\rho_o \left(R\ddot{R} + \frac{3}{2}\dot{R}^2 \right) = \left[\left(P_o - P_v + \frac{2\sigma}{R_o} \right) \left(\frac{R_o}{R} \right)^{3\kappa} + P_v \right] - \frac{2\sigma}{R} - \frac{4\mu\dot{R}}{R} - \left(P_o + P_a \sin\omega t \right) \right]$$

Inertial Terms Total Internal Pressure Total External Pressure



"Stable Cavitation"

- Repetitive pulsations about equilibrium radius
- Dominated by gas compressibility
- Larger bubbles and lower acoustic pressures
 - acoustic scattering and radiation pressure
 - acoustic emissions
 - micro-streaming, microjets, rectified diffusion





"Inertial Cavitation"

- Unstable growth -- violent collapse
- Dominated by liquid inertia
- Smaller bubbles, higher pressure
 - acoustic emissions
 - microstreaming
 - collapse jets, shock waves
 - Extreme conditions in the cavity (sonochemistry)





Radiation Stress

$$\vec{F} = - \left\langle V(t) \vec{\nabla} P \right\rangle$$



Cavitation Micro-streaming





Collapse Micro-jets





Radiated Shock Waves







Enhanced Heating



- The "nucleation threshold" is the minimum acoustic stress required to form the bubble
- In vivo cavitation nucleation thresholds are high (5-7 MPa)
 - Lack of naturally occurring nuclei
 - Cavitation field difficult to control too much damage
- Lowering the nucleation threshold makes it easier to sustain and control cavitation
 - Contrast agents
 - Superheated droplets
 - Imperfectly wetted solid microparticles



- Pulsed laser light can cavitate water.
 - Poor spatial specificity (tissue optically diffusive)
- Light absorbing nanoparticles serve as preferential site for vapor cavity formation
 - Used as contrast agents for photoacoustic imaging
- Can laser-illuminated nanoparticles serve as cavitation nucleation sites???



"Seed" tissue phantom with 40 nm gold nano-particles:

- Irradiate with pulsed laser and HIFU
- Time laser to coincide with rarefaction phase of HIFU
- Measure nucleation threshold pressure...
 - With and without laser illumination
 - As a function of laser energy





acrylimide gel phantom 15 MHz PCD (15 mm FL)

AIV AIV

> Nd:YAG laser, 532 nm (5 ns pulse) 1.1 MHz pulsed HIFU (10 cycles)



Light Only (No HIFU)



Laser nucleation threshold (no sound) ≈ 1.8 mJ/pulse HIFU nucleation threshold (no light) ≈ 4.5 MPa



0.1 mJ/pulse (3 mJ/cm²) 10 cycle acoustic pulse





Acoustic Cavitation "On Demand"





How Does it work? Energy Budget



$$E_L \equiv 0.1 \text{mJ}$$

 $\beta = 3.3$
 $R_L \equiv 0.8 \text{ mm}$
 $R_S \equiv 40 \text{ nm}$

Absorbed energy Q is roughly proportional to the laser energy E_L and the geometric cross section

$$Q = \beta \bullet E_L \bullet \left(\frac{R_s}{R_L}\right)^2$$

Q : absorbed energy

 $\beta = \beta(\lambda_L, R_S)$:

absorption efficiency

 $E_{\rm L}$: laser pulse energy

 $R_{\scriptscriptstyle S}$: particle radius

 $R_{\scriptscriptstyle L}$: laser beam radius



How Does it work? Energy Budget



δ = 14.3 nm

All absorbed energy Q is converted to heat and vaporizes a thin shell of water surrounding the particle.

$$\begin{aligned} Q &= m_{\delta} c_{v} \Delta T + m_{\delta} h_{fg} \\ m_{\delta} : \text{ mass of water shell, } c_{v} : \text{ heat capacity} \\ \Delta T &= \mathsf{T}_{\mathsf{sat}} - \mathsf{T}_{\mathsf{o}} \qquad h_{fg} : \text{ latent heat} \end{aligned}$$

 $Q = 0.87 \, pJ$

Vaporization expands the shell into a larger vapor nucleus:

$$\delta \rightarrow R_{v}$$
 (vapor shell thickness)
 R_{o} : vapor nucleus radius
 $R_{o} = R_{S} + R_{v}$

R_o = 105 nm



Parameter Study





Modeling Result

Laser: 0.1 mJ/pulse (3mJ/cm²) HIFU: 1.1MHz Nano-Particle: Gold, 40nm in radius



23



Threshold acoustic pressure reduced from 4.5 to 1 MPa Threshold laser energy reduced from 1.8 mJ to 0.1 mJ Effect well described by theory Nanoparticles can be targeted to tissue types Nanoparticles are persistent nuclei Enables cavitation nucleation "on demand"



 Broadband acoustic emissions from thermoelastic expansion of a light absorbing medium





Multispectral Imaging It's About the Hemoglobin



Blood primarily impacts local absorption

Absorption measurements yield local blood concentration

Multi-spectral absorption measurements yield oxygen saturation levels

Both are key physiological functional parameters

Prahl, Oregon Medical Laser Center, *Optical absorption of Hemoglobin* (<u>http://omlc.ogi.edu/spectra/hemoglobin/index.html</u>), 1999.



Deep tissue PA imaging requires that you get sufficient light "at depth" to excite a measureable response.

Real tissues have a lot of scattering and absorption. You can't go very deep.

Max Permissible Exposure (MPE) for 1-100 nsec pulsed laser light*:

20mJ/cm² @ 532 nm

60mJ/cm² @ 900 nm

100mJ/cm² @ 1064 nm

*American National Standard





Enhancing Photoacoustic Emissions Gold Nano-particles



- Plasmon resonant gold nano-particles are very efficient absorbers of laser energy.
- Used to enhance photoacoustic imaging techniques.
- Functionalized to targeted to specific cell populations.

• So....

*720 mJ/cm² for a 30 nm nano-particle at 532nm and 0.5 ns pulse length Lapotko, D., Opt. Express **17**(4), 2538-2556 (2009)



Ultrasound-enhanced Photoacoustic Emissions

Gold nanoparticle imbedded in target



- Introduce short laser pulse
- Photoacoustic emission from direct particle heating
- Introduce short US pulse
- Rarefaction causes small vapor "blanket" to rapidly expand and collapse
- Greatly enhances broad band emissions

US Enhanced PA Imaging





US Enhanced PA Imaging





Nanoparticles + Light (no HIFU); n = 50





Nanoparticles + Light + HIFU; n = 1





Nanoparticles + Light + HIFU; n = 1

Without HIFU

photoacoustic imaging depth

Single Shot (no averaging) at 20.8 mJ/cm² Single Shot with inertial collapse (1.5 MPa) 0.6 Filtered Detector (V) 0.6 Filtered Detector (V 0.4 0.4 0.2 0.2 -0.2 -0.2 -0.5 0.5 1.5 -0.5 0 0.5 1.5 0 Time (µs) Time (µs) By exploiting the IC emission Peak photoacoustic inertial collapse we can greatly increase

IC ≈ 35 times greater

With HIFU



Imaging by Inertial Collapse





•A 10 cycle, 1.5 MPa HIFU pulse, with a fluence of 11.4 mJ/cm²



An inertial collapse detected for approximately each acoustic cycle

Concept 2: Light-enhanced HIFU Heating





Experimental Arrangement

1.1 MHz HIFU transducer





30x30x50 mm Polyacrylamide phantom containing bovine serum albumin (BSA) and gold nanoparticles (80 nm) 7.5 MHz PCD



Experimental Protocol

- Laser: 10 Hz PRF, 10 nsec pulse length
- HIFU: Burst mode -- 1 burst per laser flash
- Burst length variable: 127 μsec 98 msec
- 60 sec exposures: P₊ ranged from 0 6 MPa
- Duty cycle varied between 0.13% & 98%







Quasi CW Exposures: Pressure Dependence



ON

OFF



Lesion Formation

LASER OFF







Two videos of single 60 s HIFU exposures with and without the laser with HIFU propagating from right to left. P_{neg} = 4.3 MPa DC = 98% Fluence = 22.6 mJ/cm²



Lesion Dimensions

Laser Fluence = 22.6 mJ/cm^2 ; DC = 98%



Nanoparticle-nucleated inertial cavitation enhances energy deposition Larger lesions result from equivalent exposure conditions



Combining US Enhanced PA Imaging and Light Enhanced HIFU Therapy

- Gel/BSA phantom
- 5x5x5 mm gel/BSA Inclusion doped with gold nano-particles
- Use US-enhanced PA to image the inclusion via raster scan

- 9 separate 60s light-enhanced HIFU exposures within the imaged inclusion
- Simulate poor HIFU targeting by making 3 exposures outside of inclusion (z=6)
- P = 2.8 MPa ; Fluence = 22.6 mJ/cm²





Conclusions & Extrapolations

- Pulsed ultrasound enables photoacoustic imaging in the presence of absorbing nanoparticles
 - x35 enhancement in PA emissions = *imaging at greater depth*
- Pulsed laser light enables controlled HIFU cavitation in the presence of absorbing nanoparticles
 - Cavitation on demand for enhanced HIFU therapy
- Lesions form only when and where light & sound & particles coexist
 - Functional particles target the tissue for both imaging and therapy
 - Relaxes the requirement for a precise, tightly focused acoustic beam
 - No optical targeting or alignment required (diffuse light)
- Could lead to targeted and controlled lesion formation in optically accessible organs
 - Breast, brain, prostate, skin
 - Catheter-based laser ablation surgery and sonothrombolysis
- An externally activated nanoparticle for targeted drug delivery?



Photoacoustically Active Nano-delivery Systems

- Porous gold nano-partices
- Nano tubes
- Light absorbing encapsulated nano-drops

Qingfeng Zhang; Nicolas Large; Peter Nordlander; Hui Wang; *J. Phys. Chem. Lett.* **2014,** 5, 370-374.

DOI: 10.1021/jz402795x

Copyright © 2014 American Chemical Society



Students: Caleb Farny Tianming Wu Puxiang Lai Henji Ju

Postdocs: Jim Mclaughlan

Collaborators: Todd Murray (Univ. of Colorado) Chuck DiMarzio (Northeastern Univ.) Robin Cleveland (Univ. of Oxford) R. Glynn Holt (Boston Univ.)







